
Simulation and Image ✧ Reconstruction for a Low-Cost ✧ PET Detector Concept

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What is PET?

- Positron Emission Tomography (PET) is one of the most **sensitive** imaging techniques available.
- It allows physicians to monitor **metabolic activity**, localise tumours and assess treatment efficacy.
- Patients are injected with a small amount of **radiotracer**, which is absorbed by metabolically active or diseased cells, making them **visible** to the scanner.

The Need for Low-Cost PET

- The World Health Organisation (WHO) has recommended a PET scanner ratio of **two scanners per million people** to meet population needs.
- South Africa currently only has **18** PET scanners for a population of nearly **60 million people**.



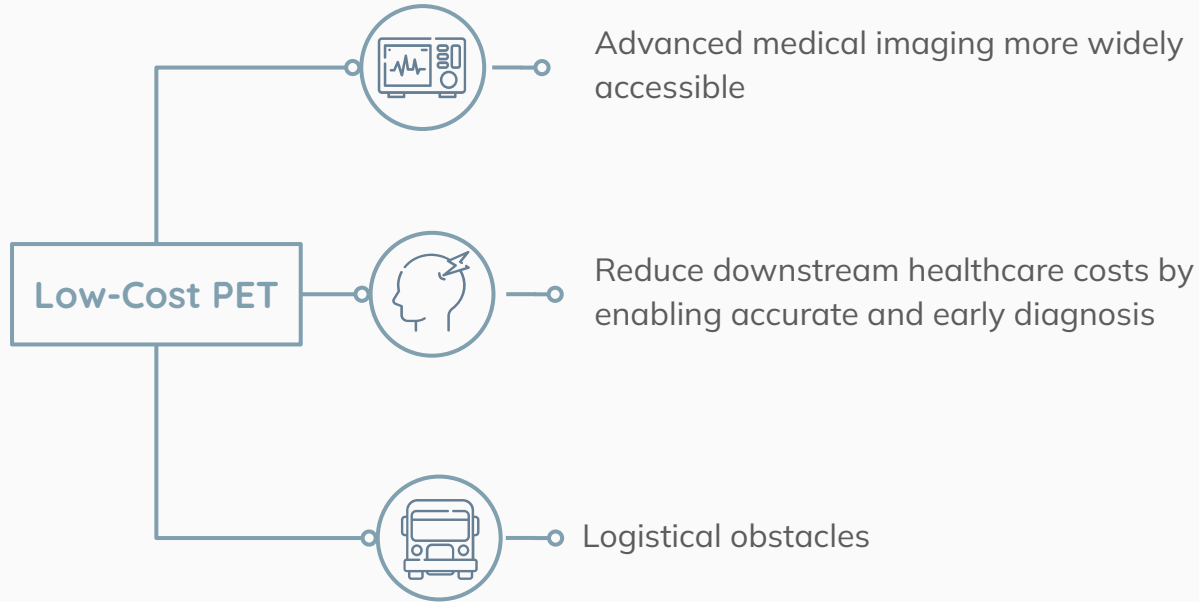
The Need for Low-Cost PET

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Private Sector
Government Sector

The Need for Low-Cost PET



Project Goals

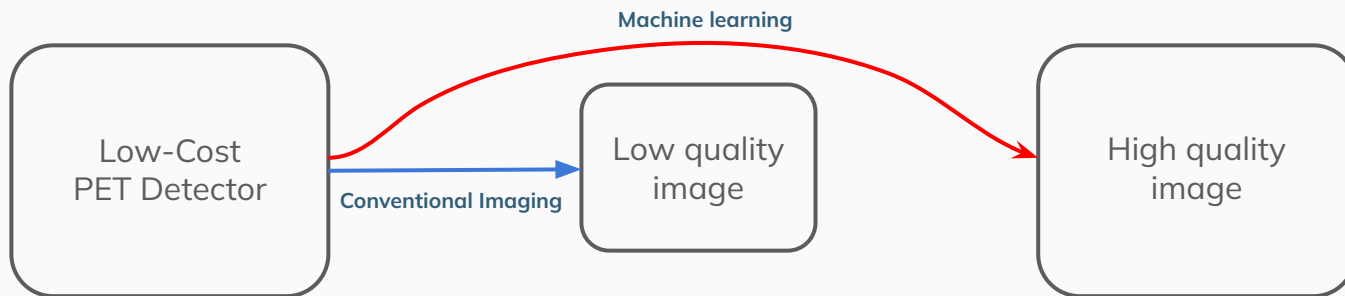
- The main goal of my project is to create a **digital workbench** through simulation to evaluate different low-cost detector designs



- At the end of this workflow, you should be able to make a suitable decision whether a low-cost detector design is **clinically usable**.

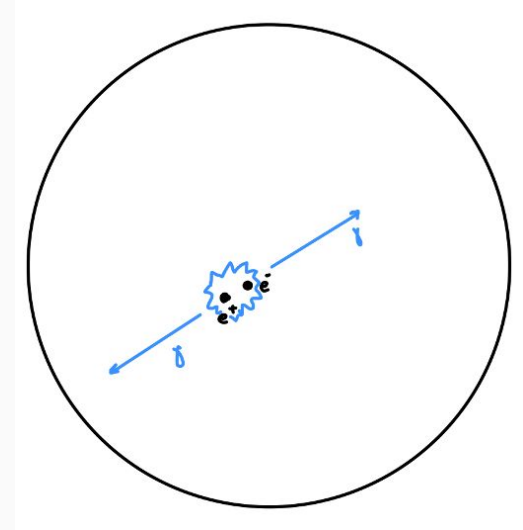
Project Goals

- If we have a **simpler** design, the images that are produced will never be of the same quality as a standard PET detector
- Can we use **machine learning** to **bridge this gap** and denoise our images to get high quality, clinically usable images?

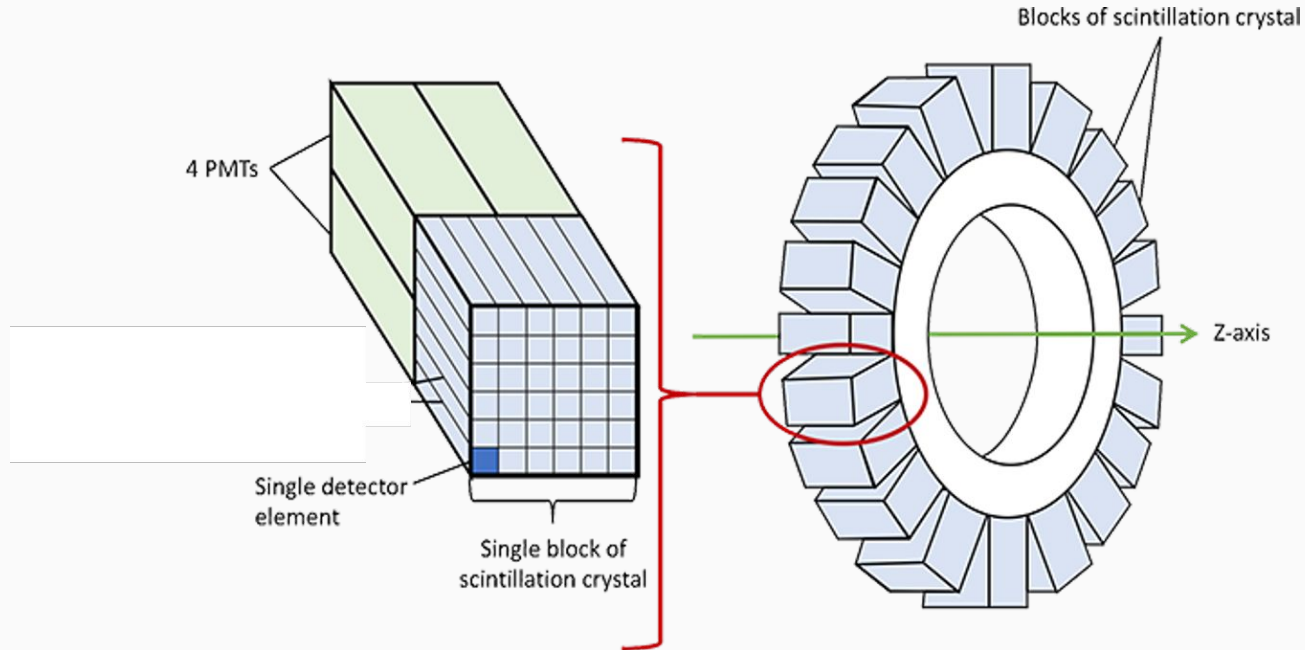


How PET Works: Annihilation

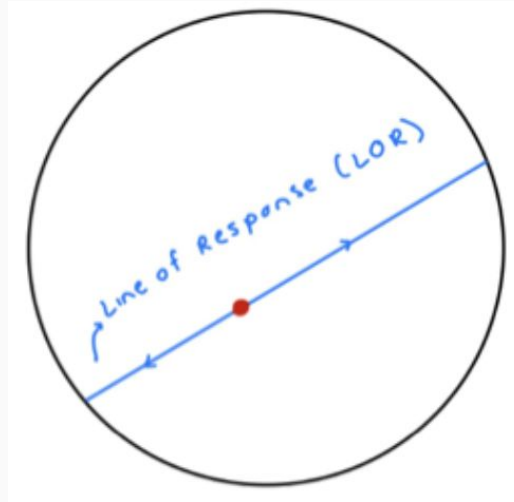
- The radiotracer that patients are injected with contain a **positron emitting isotope**
- These isotopes are **radioactive** and **unstable** and will undergo beta plus decay, **releasing a positron**, to become more stable
- When the positron encounters an electron in nearby tissue, they will undergo an **annihilation reaction**
- This reaction produces **two 511 keV photons** which move to **opposite sides** of the detector



How PET Works: Detection



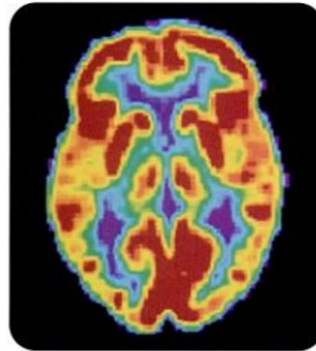
How PET Works: Detection



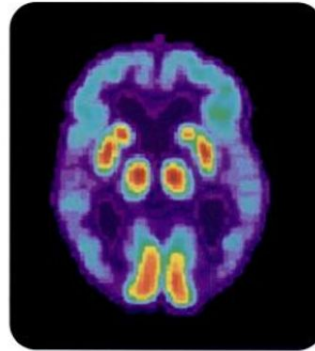
- The LOR only constrains the annihilation event to lie somewhere along that line; **it does not indicate the exact location of the event.**

How PET Works: Image Reconstruction

- The primary task of an image reconstruction algorithm for a PET detector is to take the data collected and **transform it into an accurate image**



PET Scan of Normal Brain



PET Scan of Alzheimer's Disease Brain



From Design to Decision: Design

Detector Design



Simulation



Image Reconstruction



Comparison Metrics



Final Decision





Detector Design

- The first preliminary design that has been tested is a compact PET system with **simplified modules** and **smaller geometry**
- This will be compared with a **commercial Philips Vereos Digital PET system**

	Philips Vereos	Low-Cost
Radius	500 mm	160 mm
Module Dimensions	19 mm x 131.4 mm x 164 mm	15 mm x 24 mm x 24 mm
Pixels per module	1280	64

**A module is an array of scintillators*



From Design to Decision: Simulation

Detector Design



Image Reconstruction



Final Decision



Simulation



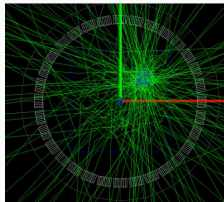
Comparison Metrics



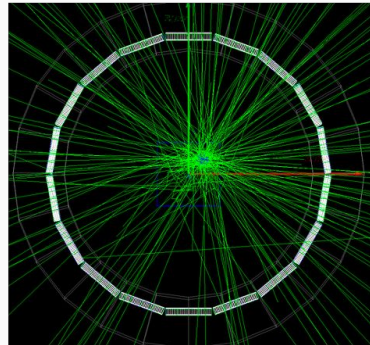
The Simulation

- The simulations in this project were performed using **GATE** (Geant4 Application for Tomographic Emission)
- GATE builds on the Geant4 Monte Carlo toolkit and provides a dedicated interface for **medical imaging simulations**

Visualisation of the compact low-cost PET scanner in GATE

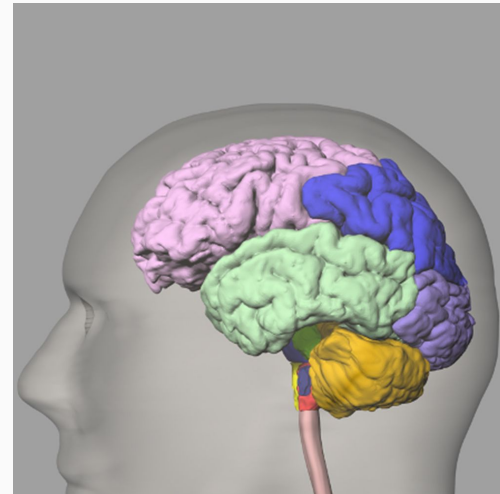


Visualisation of the Philips Vereos PET scanner in GATE



Phantoms

- Phantoms are objects that are used to **mimic human tissue** to validate detector performance
- GATE provides the flexibility to **define various phantoms** with controlled activity distributions
- Realistic brain phantoms can be created by **voxelising public CT scan datasets** into anatomical regions



Example of a voxel-based brain phantom segmenting ~100 structures generated from CT/MRI data and voxelised for use in GATE.

What does it Mean to Voxelise Something?

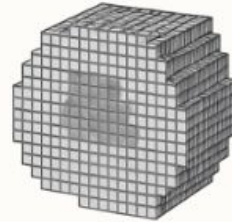
- **Voxelisation:** The process of converting a 3D object into a grid of voxels



*A single 2D example
of a CT brain scan*



Stacking the slices



*Each voxel stores local
tissue information*



*Voxelised phantoms
used in PET simulation*



From Design to Decision: Image Reconstruction

Detector Design



Simulation

Image Reconstruction



Comparison Metrics

Final Decision

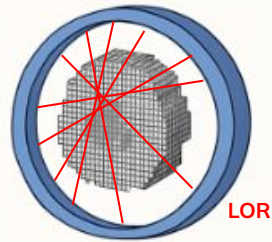




Image Reconstruction Using MLEM

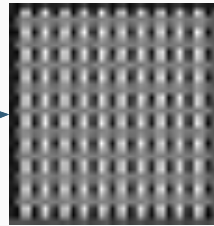
- We use the **Maximum Likelihood Expectation Minimisation (MLEM)** algorithm for image reconstruction
- MLEM is the **most widely used** method in PET imaging
- MLEM tries to find the **most likely image** that would have been produced the data that we measured

Image Reconstruction Using MLEM

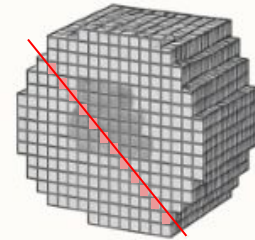


LOR

Collecting the data



Start with a guess



Forward project: Simulate the detectors view

Correct and
improve image

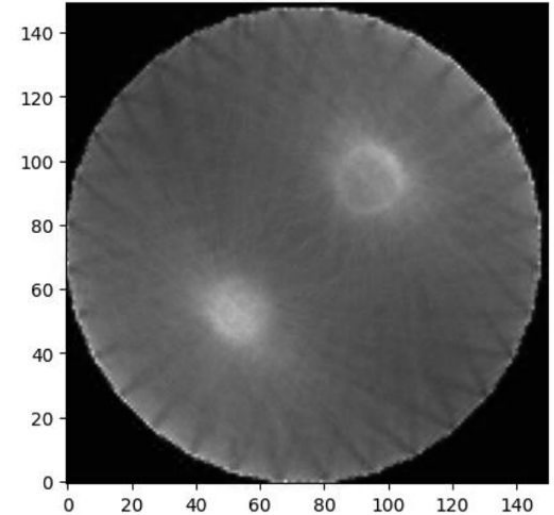
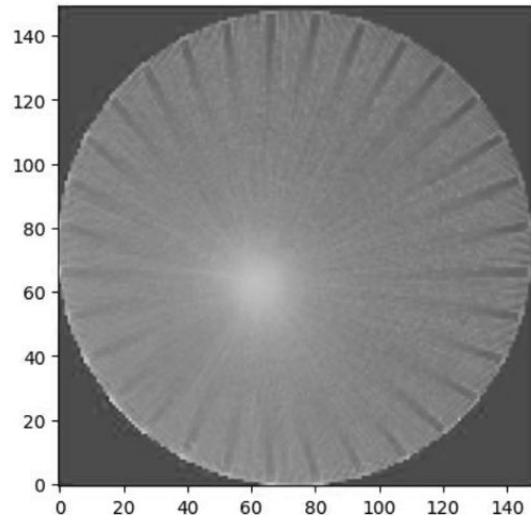
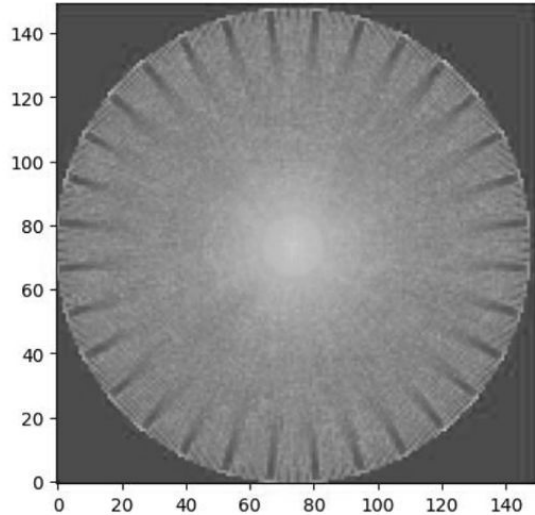
$$L(D|P(I))$$

D: Measured Data
P(I): Forward projection
of image estimate I

We evaluate the likelihood of the
measured data given our current guess



Image Reconstruction Using MLEM



Reconstructed images of spherical sources using MLEM



From Design to Decision: Comparison Metrics

Detector Design



Simulation

Image Reconstruction



Comparison Metrics

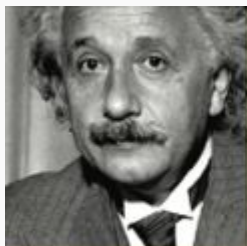
Final Decision



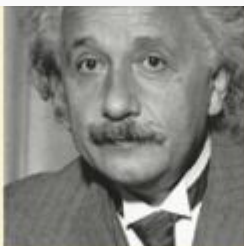


Image Comparison Metrics

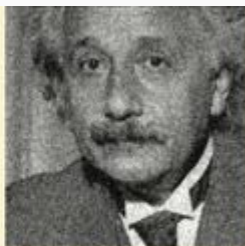
- We need a metric that is able to quantify how **similar** the images produced by the detectors are
- **Mean squared error (MSE)** has been shown to report nearly **identical values** for images that appear very **different** to the human eye



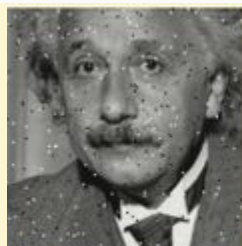
MSE=306, SSIM=0.928
CW-SSIM=0.938



MSE=309, SSIM=0.987
CW-SSIM=1.000



MSE=309, SSIM=0.576
CW-SSIM=0.814



MSE=313, SSIM=0.730
CW-SSIM=0.811



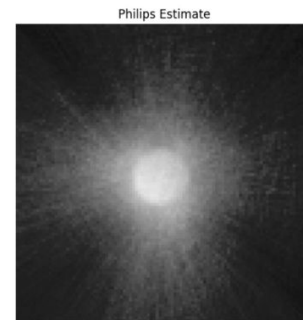
MSE=309, SSIM=0.580
CW-SSIM=0.633



MSE=308, SSIM=0.641
CW-SSIM=0.603

The Structural Similarity Index (SSIM)

- The core idea behind the SSIM is that the human visual system is highly sensitive to structural changes, and therefore the **image quality should be assessed based on the preservation of structural information**
- The SSIM evaluates the similarity between two images based on three components: **luminance, contrast and structure**
- The SSIM score ranges from -1 to 1 where a value of **1** indicates perfect structural similarity



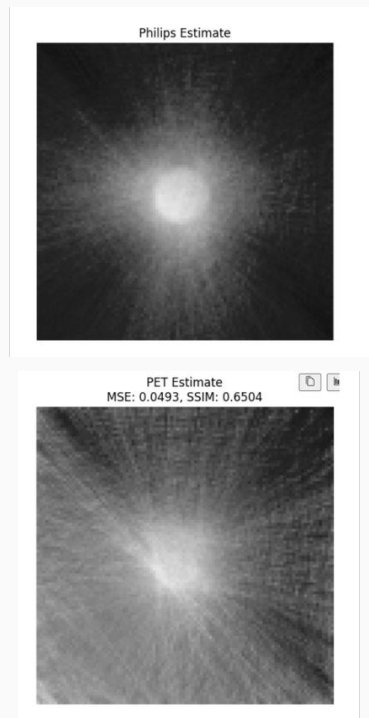
*Reconstructed Image
using Vereos Detector*



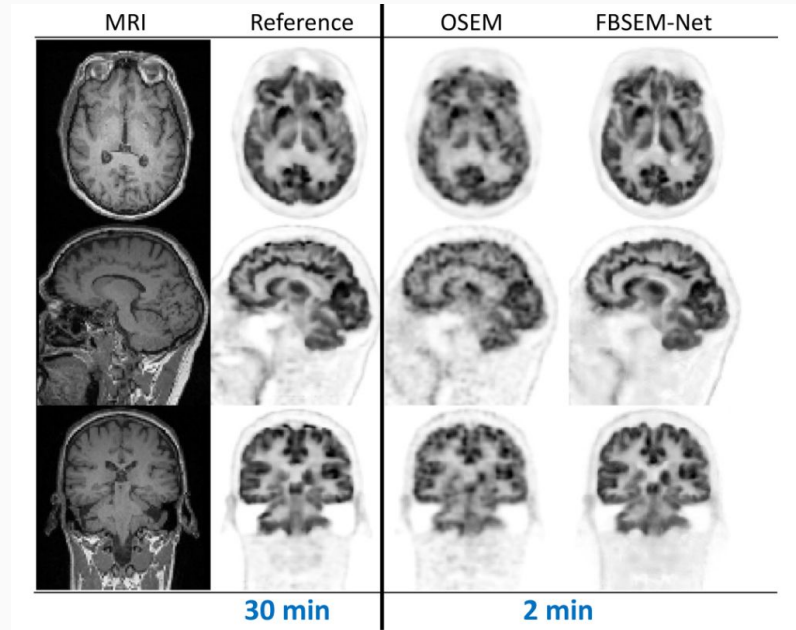
*Reconstructed Image
using low-cost detector,
with the relevant SSIM
score*

Using ML to Bridge the Image Quality Gap

- The simplified modules and reduced resolution of our design lead to inherently **noisier, lower quality images**
- We are implementing ML denoising methods to **enhance image quality**, aiming to approach the performance of high-end PET systems.
- These include autoencoders trained on high-resolution data to **learn structural priors** for image upsampling and denoising.



Using ML to Bridge the Image Quality Gap



Machine learning enhances low-count PET scans: A deep learning model (FBSEM-Net) reconstructs high-quality images from 2-minute scans, recovering structural detail comparable to a 30-minute reference.



Scaling Up the Simulation

	Current Simulation	Real PET Brain Scan
Scan time	0.1 s	20 minutes
Photon pairs detected	~500 000	~10 ¹¹
% of full data	0.0005%	100%

- To simulate realistic scan duration and photon statistics we need to **optimise our workflow**

Making the Final Decision

Detector Design



Image Reconstruction



Simulation



Comparison Metrics



Final Decision



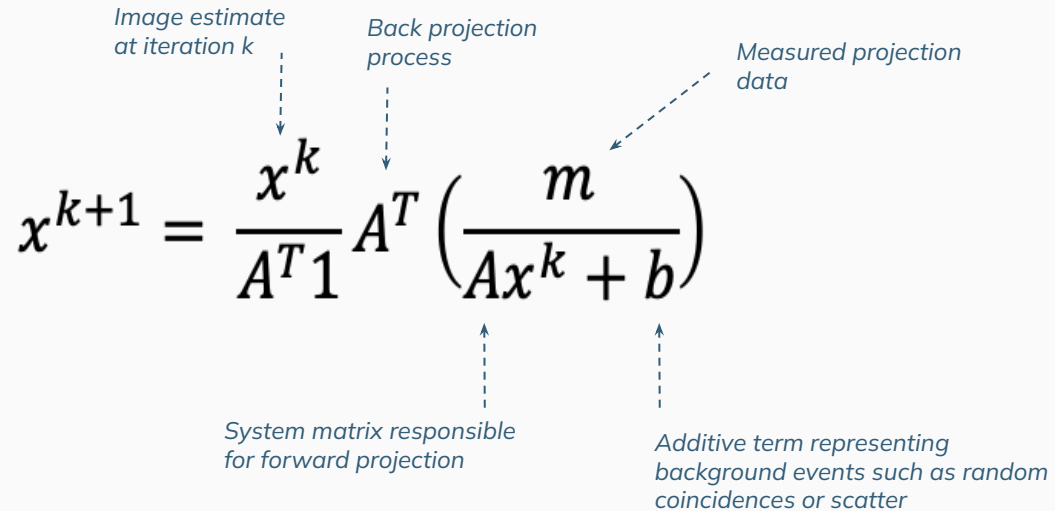
- By running each design through this pipeline, we can make an informed decision about:
 - *Is the design producing clinically relevant images?*
 - *Is the performance good enough to replace high-cost systems?*

Thank you!

Do you have any questions?



The MLEM Update Equation



The diagram illustrates the MLEM Update Equation with the following components and annotations:

- Equation:**
$$x^{k+1} = \frac{x^k}{A^T 1} A^T \left(\frac{m}{Ax^k + b} \right)$$
- Annotations:**
 - Image estimate at iteration k* points to x^k .
 - Back projection process* points to A^T .
 - Measured projection data* points to m .
 - System matrix responsible for forward projection* points to A .
 - Additive term representing background events such as random coincidences or scatter* points to b .

